

**MICROPARTICLE PROTECTION
OF THERAPEUTIC AGENTS**

STATEMENT OF RELATED APPLICATIONS

[0001] This application is related to U.S. Serial No. 09/429,178 filed October 28, 1999 and entitled "Biocompatible Medical Devices". This application is also related to U.S. Serial No. 09/503,586 filed February 14, 2000, also entitled "Biocompatible Medical Devices". Each of these applications is hereby incorporated by reference in its entirety.

FIELD OF THE INVENTION

[0002] This invention relates to the protection of therapeutic agents and more particularly to novel techniques and compositions for the protection of therapeutic agents using microparticles.

BACKGROUND OF THE INVENTION

[0003] As noted in related U.S. Serial Nos. 09/429,178 and 09/503,586, devices having metallic and polymeric components are used extensively in the medical field. In many cases, such medical devices are used for delivery of a solution or suspension containing a pharmaceutically active agent, and the pharmaceutically active agent comes into contact with the metallic or polymeric component during the course of its delivery. Metallic materials used in such devices include stainless steel and nickel-titanium superelastic alloys (e.g., nitinol). Polymeric components used in such devices include polycarbonate, polyimide, acrylonitrile/butadiene/styrene resins (ABS), poly ether ether ketone (PEEK), epoxy-based adhesives (such as FDA2 or FDA23) and nylon (such as nylon 6,6). The inventors in related U.S. Serial Nos. 09/429,178 and 09/503,586 have found, however, that despite their reputation as being substantially inert, such materials can be incompatible to varying degrees with certain pharmaceutically active agents.

[0004] The present invention provides a simple and unexpected way of overcoming the above and other incompatibilities.

SUMMARY OF THE INVENTION

[0005] According to an embodiment of the present invention, a method is provided in which microparticles are used to protect the pharmaceutical effectiveness of a pharmaceutically active agent. The method comprises: (a) providing a pharmaceutically acceptable suspension comprising the pharmaceutically active agent and microparticles; and (b) exposing the pharmaceutically acceptable suspension to a component or condition that is incompatible with the pharmaceutically active agent, such that the microparticles result in a pharmaceutical effectiveness of the pharmaceutically active agent that is greater than it would have been in the absence of the microparticles. Preferably, the microparticles result in a pharmaceutical effectiveness of the pharmaceutically active agent that is at least 10% greater than the pharmaceutical effectiveness of the pharmaceutically active agent would have been in the absence of the microparticles.

[0006] Components incompatible with the pharmaceutically active agent include metals (such as certain stainless steel and nickel-titanium alloys), polymers (such as certain poly ether ether ketones, polyimides, epoxies, nylons, acrylonitrile/butadiene/styrene polymers and polycarbonates) and glass.

[0007] Conditions incompatible with the pharmaceutically active agent include freeze-thaw transformations.

[0008] The microparticles preferably range from 0.01 to 100 microns in largest dimension, more preferably 0.1 to 10 microns in largest dimension. The microparticles are preferably provided in an amount ranging from 0.1 to 1 wt% within the suspension. Polymer microparticles, such as polystyrene microparticles, are one preferred class of microparticles.

[0009] According to another embodiment of the invention, a method of treatment is provided. The method comprises: (a) providing a pharmaceutically acceptable suspension comprising a pharmaceutically active agent and microparticles; (b) providing a medical device having a component that is incompatible with the pharmaceutically active agent; and (c) parenterally injecting

the pharmaceutically active agent into a patient via the device while at the same time removing the microparticles from the pharmaceutically acceptable suspension. Preferred devices include parenteral injection devices, such as vascular catheters and syringes.

[0010] According to another embodiment of the invention, a device for parenteral injection is provided that comprises: (a) a pharmaceutically acceptable suspension comprising a pharmaceutically active agent and microparticles; (b) a device component that contacts the suspension and is incompatible with the pharmaceutically active agent; and (c) a separator that acts to remove the microparticles from the pharmaceutically acceptable suspension prior to parenteral injection.

[0011] According to another embodiment of the invention, a pharmaceutically acceptable suspension is provided. The suspension comprises: (a) a pharmaceutically active agent; and (b) microparticles that prevent a substantial reduction in pharmaceutical effectiveness of the pharmaceutically active agent upon being exposed to a material or condition that is incompatible with the pharmaceutically active agent.

[0012] One advantage associated with the present invention is that the efficacy of pharmaceutically active agents can be protected in a simple manner.

[0013] Another advantage of the present invention is that a pharmaceutically active agent can be stored in a storage container or delivered from a medical device that contains materials that would otherwise result in a substantial reduction in the pharmaceutical effectiveness of the pharmaceutically active agent.

[0014] Another advantage of the present invention is that a pharmaceutically active agent can be stored under conditions that would otherwise result in a substantial reduction in the pharmaceutical effectiveness of the pharmaceutically active agent.

[0015] Yet another advantage of the present invention is that an agent (i.e., microparticles) can be provided to protect the efficacy of the pharmaceutically active agent, but need not be introduced into a patient at the time of administration.

BRIEF DESCRIPTION OF THE DRAWINGS

DETAILED DESCRIPTION

[0019] By “pharmaceutical effectiveness” or “pharmaceutical efficacy” is meant any desired pharmaceutical result. As a specific example, the pharmaceutical effectiveness of a virus can be measured by the ability of that virus to infect cells. As another example, the pharmaceutical effectiveness of a protein can be measured by its activity within an ELISA assay.

[0021] Pharmaceutical effectiveness is said to be “substantially increased”, is “substantially higher” or is said to undergo a “substantial increase” when it is increased, for example, by at least 5%, more commonly 10%, 20%, 30%, 40%, 50% or more.

[0022] At present, many pharmaceutical articles, including various medical devices, are known in which solutions or dispersions of pharmaceutically active agents come into contact with materials prior to delivery to the body. However, as seen below in the Examples, and as further shown in related U.S. Serial Nos. 09/429,178 and 09/503,586, where certain pharmaceutically active agents contact substrates comprising certain materials, their pharmaceutical effectiveness is substantially reduced.

[0023] For instance, it has been found that where viral particles contact certain metallic materials, such as certain stainless steel and/or nickel-titanium alloys (e.g., nitinol), or they contact certain polymeric materials, such as certain poly ether ether ketones (PEEK), polyimides, epoxies, nylons, acrylonitrile/butadiene/styrene resins (ABS) and/or polycarbonates, viral transfection may be substantially reduced. This is surprising, since it is normally assumed that such metallic and polymeric materials are substantially inert and hence unlikely to adversely affect pharmaceutically active agents.

[0024] The present invention overcomes these and other difficulties through the use of microparticles that substantially protect the pharmaceutical effectiveness of pharmaceutically active agents upon encountering materials or conditions that are incompatible with the active agents.

[0025] It is well within the skill of those of ordinary skill in the art to determine which materials, in addition to those specifically listed above, are incompatible with a given pharmaceutically active agent. Possible mechanisms for a substantial reduction in pharmaceutical effectiveness include inactivation (e.g., through denaturation, precipitation, damage, and so forth) and adsorption of the pharmaceutically active agent. It is also well within the skill of those of ordinary skill in the art to determine which conditions are incompatible with a given pharmaceutically active agent.

[0026] The present invention utilizes microparticles to substantially protect the pharmaceutical effectiveness of pharmaceutically active agents upon contacting incompatible materials or encountering incompatible conditions. The

microparticles and the pharmaceutically active agent are preferably provided in a suspension. As a result of the presence of the microparticles in the suspension, the pharmaceutically active agent is substantially protected upon contact with the incompatible materials or exposure to the incompatible conditions.

[0027] By "substantially protected" is meant that effectiveness of the pharmaceutically active agent is substantially greater in the presence of the microparticles, relative to the effectiveness of the pharmaceutically active agent in the absence of the microparticles.

[0028] The microparticles of the present invention can be made of essentially any material that is effective to achieve protection of the pharmaceutically active agent, without resulting in a pharmaceutically unacceptable outcome (e.g., unacceptable levels of toxicity). These materials include materials that are not incompatible with the pharmaceutically active agent, including certain metals (e.g., gold, titanium and platinum), ceramics/glasses (e.g., quartz), polymers, and combinations of the same.

[0029] Polymers appropriate for the practice of the invention may be crosslinked or uncrosslinked, linear or branched, natural or synthetic, thermoplastic or thermosetting, or biostable, biodegradable, bioabsorbable or dissolvable.

[0030] Exemplary polymers include the following polymers and copolymers: polycarboxylic acid polymers and copolymers including polyacrylic acids (e.g., acrylic latex dispersions and various polyacrylic acid products such as HYDROPLUS, available from Boston Scientific Corporation, Natick Mass. and described in U.S. Patent No. 5,091,205, the disclosure of which is hereby incorporated herein by reference, and HYDROPASS, also available from Boston Scientific Corporation); acetal polymers and copolymers; acrylate and methacrylate polymers and copolymers; cellulosic polymers and copolymers, including cellulose acetates, cellulose nitrates, cellulose propionates, cellulose acetate butyrates, cellophanes, rayons, rayon triacetates, and cellulose ethers such as carboxymethyl celluloses and hydroxyalkyl celluloses; polyoxymethylene polymers and copolymers; polyimide polymers and copolymers such as polyether block imides,

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methacrylate copolymers and ethylene-vinyl acetate copolymers; fluorinated polymers and copolymers, including polytetrafluoroethylenes (PTFE), poly(tetrafluoroethylene-co-hexafluoropropene) (FEP), modified ethylene-tetrafluoroethylene copolymers (ETFE), and polyvinylidene fluorides (PVDF); silicone polymers and copolymers; polyurethanes (e.g., BAYHYDROL polyurethane dispersions); p-xylylene polymers; polyiminocarbonates; copoly(ether-esters) such as polyethylene oxide-polylactic acid copolymers; polyphosphazines; polyalkylene oxalates; polyoxaamides and polyoxaesters (including those containing amines and/or amido groups); polyorthoesters; biopolymers, such as polypeptides, proteins, polysaccharides and fatty acids (and esters thereof), including fibrin, fibrinogen, collagen, elastin, chitosan, gelatin, starch, glycosaminoglycans such as hyaluronic acid; as well as blends and copolymers of the same.

[0031] Those of ordinary skill in the art will be able to determine which polymers are most appropriate for a given pharmaceutically active material with relative ease using, for example, techniques like those used in the Examples.

[0032] Latex beads represent one preferred class of polymer microparticles that are useful in connection with the present invention. Natural latexes as well as synthetic latexes (e.g., latexes formed by emulsion polymerization from polystyrene, styrene-butadiene copolymers, acrylate polymers, polyvinyl acetate, and so forth) are preferred, with polystyrene latexes being more preferred.

[0033] The term "microparticle" as used herein refers to small particles ranging in largest dimension from 0.01 to 1000 microns, preferably 0.01 to 100 microns, more preferably 0.1 to 10 microns, and even more preferably about 1 micron. While substantially spherical particles (including both spheres and beads) are preferred, particles of any shape, including rod-shaped particles and irregularly shaped particles, are contemplated.

[0034] The microparticles and pharmaceutically active agents are provided within any physiologically acceptable liquid medium known in the art, including physiological saline, phosphate buffered saline, and solutions containing trehalose,

sucrose, glycerol, tris(hydroxymethyl)aminomethane buffer and/or MgCl_2 .

Additional adjuvants known in the art are also contemplated.

[0035] Preferred amounts of the microparticles range from 0.01 to 10 wt% within the suspension, more preferably 0.1 to 1 wt%.

[0036] Preferred amounts of the pharmaceutically active agents are therapeutically effective amounts; such amounts are well within the ability of those of ordinary skill in the art to determine.

[0037] "Pharmaceutically active agents", "pharmaceutically active materials", "therapeutic agents", "drugs" and other related terms are used interchangeably herein and include genetic therapeutic agents, non-genetic therapeutic agents and cells. Pharmaceutically active agents useful in accordance with the present invention may be used singly or in combination.

[0038] Therapeutic agents include cells of human origin (autologous or allogeneic), including stem cells, or from an animal source (xenogeneic), which can be genetically engineered if desired to deliver proteins of interest. Cell types include bone marrow stromal cells, endothelial progenitor cells, myogenic cells including cardiomyogenic cells such as procardiomyocytes, cardiomyocytes, myoblasts such as skeletomyoblasts, fibroblasts, stem cells (e.g., mesenchymal, hematopoietic, neuronal and so forth), pluripotent stem cells, macrophage, satellite cells and so forth. Cells appropriate for the practice of the present invention also include biopsy samples for direct use (e.g., whole bone marrow) or fractions thereof (e.g., bone marrow stroma, bone marrow fractionation for separation of leukocytes). Where appropriate, media can be formulated as needed to maintain cell function and viability.

[0039] Therapeutic agents also include both polymeric (e.g., proteins, enzymes) and non-polymeric (e.g., small molecule therapeutics) agents and include Ca-channel blockers, serotonin pathway modulators, cyclic nucleotide pathway agents, catecholamine modulators, endothelin receptor antagonists, nitric oxide donors/releasing molecules, anesthetic agents, ACE inhibitors, ATII-receptor antagonists, platelet adhesion inhibitors, platelet aggregation inhibitors, coagulation

pathway modulators, cyclooxygenase pathway inhibitors, natural and synthetic corticosteroids, lipoxigenase pathway inhibitors, leukotriene receptor antagonists, antagonists of E- and P-selectins, inhibitors of VCAM-1 and ICAM-1 interactions, prostaglandins and analogs thereof, macrophage activation preventers, HMG-CoA reductase inhibitors, fish oils and omega-3-fatty acids, free-radical scavengers/antioxidants, agents affecting various growth factors (including FGF pathway agents, PDGF receptor antagonists, IGF pathway agents, TGF- β pathway agents, EGF pathway agents, TNF- α pathway agents, Thromboxane A2 [TXA2] pathway modulators, and protein tyrosine kinase inhibitors), MMP pathway inhibitors, cell motility inhibitors, anti-inflammatory agents, antiproliferative/antineoplastic agents, matrix deposition/organization pathway inhibitors, endothelialization facilitators, blood rheology modulators, as well as integrins, chemokines, cytokines and growth factors.

[0040] Therapeutic agents also include genetic therapeutic agents and proteins, such as ribozymes, anti-sense polynucleotides and polynucleotides coding for a specific product (including recombinant nucleic acids) such as genomic DNA, cDNA, or RNA. The polynucleotide can be provided in "naked" form or in connection with vector systems that enhances uptake and expression of polynucleotides. These can include DNA compacting agents (such as histones), non-infectious vectors (such as plasmids, lipids, liposomes, cationic polymers and cationic lipids) and viral vectors such as viruses and virus-like particles (i.e., synthetic particles made to act like viruses). The vector may further have attached peptide targeting sequences, antisense nucleic acids, and DNA chimeras which include gene sequences encoding for ferry proteins such as membrane translocating sequences ("MTS") and herpes simplex virus-1 ("VP22").

[0041] Further therapeutic agents include:

- o Anti-sense DNA and RNA
- o tRNA or rRNA to replace defective or deficient endogenous molecules
- o Gene delivery agents, which may be either endogenously or exogenously controlled. Examples of endogenous control include promoters that are sensitive

to a physiological signal such as hypoxia or glucose elevation. Exogenous control systems involve gene expression controlled by administering a small molecule drug. Examples include tetracycline, doxycycline, ecdysone and its analogs, RU486, chemical dimerizers such as rapamycin and its analogs, etc.

- o Angiogenic molecules including:
 - o growth factors: such as acidic and basic fibroblast growth factors, vascular endothelial growth factor, epidermal growth factor, transforming growth factor alpha and beta, platelet-derived endothelial growth factor, platelet-derived growth factor, platelet derived endothelial cell growth factor, tumor necrosis factor α , hepatocyte growth factor, insulin like growth factor, placental growth factor; PR39, angiogenin, prostaglandin E1 and E2, interleukin 8, angiopoietins (I, II, III, IV, etc), androgens, proliferin, granulocyte colony stimulating factor, estrogens
 - o transcription factors: such as Hif1a, Dell1,
 - o protein kinases: such as Akt
- o Cytotoxic factors or cell cycle inhibitors, including CD inhibitors: such as p53, thymidine kinase ("TK") and other agents useful for interfering with cell proliferation
- o The family of bone morphogenic proteins ("BMP's"): including BMP-2, BMP-3, BMP-4, BMP-5, BMP-6 (Vgr-1), BMP-7 (OP-1), BMP-8, BMP-9, BMP-10, BMP-11, BMP-12, BMP-13, BMP-14, BMP-15, and BMP-16. Currently preferred BMP's are any of BMP-2, BMP-3, BMP-4, BMP-5, BMP-6 and BMP-7. These dimeric proteins can be provided as homodimers, heterodimers, or combinations thereof, alone or together with other molecules. Alternatively or, in addition, molecules capable of inducing an upstream or downstream effect of a BMP can be provided. Such molecules include any of the "hedgehog" proteins, or the DNA's encoding them.
- o Cell survival molecules: including Akt, insulin-like growth factor 1, NF-kB decoys, I-kB,

- [0042]** A "polynucleotide" is a nucleic acid molecule polymer, such as DNA, RNA and their analogs, having as few as 3 nucleotides, and can include both double- and single-stranded sequences. A "protein" is a polymer of as few as two (dimer) amino acid residues.

[0044] To form the suspensions of the present invention, the microparticles and

the pharmaceutically active agent are commingled in a liquid medium by essentially any known means, including stirring, shaking, and so forth.

[0045] After commingling, the suspension containing the microparticles and the pharmaceutically active agent can be stored in any manner known in the art. In one preferred embodiment, the suspension is stored in an ampoule (i.e., a sealed container, typically glass or plastic, which contains a sterile solution for parenteral injection) until the time of administration.

[0046] The use of the microparticle suspensions of the present invention with (a) manufacturing articles, including fermentors, glassware, plasticware, probes and tubing, (b) other storage and transport articles, including storage vessels, transport vessels, stoppers, lids and septums, and (c) analytical articles, including needles, pipette tips, cell culture apparatus and analytical equipment, is also contemplated.

[0047] Where the therapeutic agent is in solution or is substantially smaller than the microparticles used, separation of the therapeutic agent and microparticles can be carried out with relative ease. For example, the microparticles can be separated from the therapeutic agent by straining the microparticles from the suspension, for example, by passing the suspension through a filter of an appropriate pore size (or, as another example, through a screen of appropriate mesh) prior to administration to a patient. Preferred patients are mammalian patients, more preferably human patients.

[0048] For instance, as set forth in the Examples below, the addition of 1-micron polystyrene latex beads to a virus suspension has been shown to essentially retain virus activity when exposed to an incompatible material. In these Examples, the beads are on the order of 10 times the size of the viral particles. As a result of this large size differential, the polymeric beads can be easily excluded from an injectate by placing a size exclusion mesh at the distal end of a delivery lumen, permitting injection of the viral particles without injection of the polymeric beads. Similarly, where loss of activity is related to storage and where the medical device is not incompatible with the therapeutic agent, the beads can be separated prior to association of the therapeutic agent with the medical device.

[0049] Alternatively, by selecting biocompatible microparticles, the microparticles can be administered to a patient along with the therapeutic agent. Referring again to the Examples below, the latex polystyrene beads are tissue compatible and may be injected along with the viral particles to the patient. Injection of the beads is believed to enhance both cellular gene transfer and in vivo stability.

[0050] In many preferred embodiments of the present invention, the microparticle suspensions are administered to patients via drug-delivery medical devices and accessories. Contemplated medical devices are numerous. For example, the medical devices contemplated for use in connection with the present invention can be those used for systemic treatment or those used for local treatment of a tissue or organ. Non-limiting examples include tumors; organs including but not limited to the heart, lung, brain, liver, kidney, bladder, urethra and ureters, eye, intestines, stomach, pancreas, ovary, and prostate; skeletal muscle; smooth muscle; breast; cartilage; and bone.

[0051] Essentially any medical device for parenteral injection (i.e., administration by a route other than the alimentary canal, including subcutaneous, intramuscular, intravenous, intravascular, intraorbital, intracapsular, intraspinal and intrasternal administration) is contemplated for use in connection with the present invention.

[0052] Preferred medical devices include catheters, including endoluminal catheters such as needle injection catheters (e.g., for endocardial, epicardial, and pericardial agent administration), balloon catheters, diagnostic catheters and perfusion catheters, conventional needle syringes, hypodermic needles, intravenous injection devices, biopsy needles and devices, tissue ablation devices, aspirating needles, stents, and so forth. Specific examples of devices for drug delivery to the heart include, for example, those found in the following patents and patent applications: US 5,450,846, US 5,840,059, US 5,878,751, US 5,551,427, US 5,931,834, US 5,925,012, US 5,925,033, US 5,538,504, WO 99/39624, WO

99/44656, WO 99/21510, WO 99/29251, EP A 99-06 0895752, and EP A 99-01 0888750, each of which is incorporated herein by reference.

[0053] In some cases, the microparticles are provided because the entire medical device is composed of an incompatible material. In other cases, only a portion of the medical device is composed of such incompatible materials.

[0054] The present invention is particularly useful in connection with viral delivery from percutaneous transcatheter devices.

[0055] In other preferred embodiments of the present invention, the microparticles are used to protect the effectiveness of pharmaceutically active agents under conditions related to storage. For example, the microparticles can be used to protect the activity of virus suspensions during storage and during freeze-thaw.

[0056] Below are Examples directed to a specific embodiment for carrying out the present invention. The Examples are offered for illustrative purposes only, and are not intended to limit the scope of the present invention in any way.

[0057] The Examples are directed to the protection of adenoviral vectors. Adenoviral vectors are a highly efficient way to transfer genetic material. Systemic delivery of adenoviral vectors is not preferable due to non-target organ infection. On the other hand, administration of adenovirus gene therapies using a medical device platform provides a means of site-specific delivery with minimal systemic leakage. However, vector instability persists as a major limitation of this strategy. Specifically, as noted in U.S. Serial No. 09/429,178 and U.S. Serial No. 09/503,586, medical devices have been shown to negatively impact adenoviral activity. See also Marshall et al., Molecular Therapy 2000, 1(5): 423-429.

EXAMPLE 1

[0058] A CMV-*LacZ* adenovirus (i.e., an adenoviral vector driven by a cytomegalovirus promoter and β -galactosidase reporter gene based on the *LacZ* enzyme) is used as a stock virus in this example.

[0059] An adenoviral solution having an Ad_{CMV-LacZ} titer of 1×10^9 functional units

[0060] At the same time a suspension is prepared by combining the following:
(a) 90 vol% adenoviral solution at a titer appropriate to give a final titer of 1×10^9 fu/ml and (b) 10 vol% Fluoresbrite™ YG Microspheres from Polysciences Inc., which contains 1.0-micron fluorescent polystyrene beads at a concentration of 2.5% solids in water. This combination results in a suspension that contains a final adenovirus titer of 1×10^9 fu/ml as well as 0.25% solids as microspheres (due to the 10:1 dilution of the bead solution).

[0062] Catheter effluents were then collected and titered on HeLa cells (human epidermoid carcinoma cells). For this purpose, HeLa cells were first plated out in well plates at 70% confluency the day before the experiment. Prior to contacting the HeLa cells, the viral solution was diluted appropriately in infection media (Dulbecco's Modified Eagle's Medium + 2% Fetal Bovine Serum) to achieve a result of 100 to 1000 infected cells per well. The diluted virus was added to the HeLa cells in the wells and incubated at 37°C for 1 hour. 5 mls of DMEM + 10% FBS were then added to each well, followed by incubation for 24-30 hours at 37°C. After aspiration of the media, the cells were fixed in 0.5% glutaraldehyde in PBS (phosphate buffered saline) for 10 minutes. The cells were washed twice in PBS and stained using an X-gal staining solution overnight at 37°C (X-gal is 5-bromo-4-chloro-3-indolyl- β -D-galactoside, which is hydrolyzed by β -galactosidase to form a blue product). Blue cells (i.e., galactosidase-positive cells) were counted the next day to determine the titer.

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conditions. The results for both the adenoviral solution and the adenoviral/bead suspension are presented in Fig. 1. As can be seen, incubation of the adenovirus solution within the Stiletto™ catheter leads to an essentially complete loss of virus activity. In contrast, the addition of 1 micron polystyrene latex beads to the adenovirus solution results in an essentially complete retention of virus activity.

EXAMPLE 2

[0064] Efficacy of adenovirus delivery from a standard needle was performed in a mouse model. An adenoviral solution and an adenoviral suspension containing beads (10 vol% Fluoresbrite™ YG Microspheres), each having an Ad_{CMV-LacZ} titer of 10⁸fu/50μl, were prepared. Mice were anesthetized and a left thoracotomy was used to expose the heart. Direct epicardial injections (1 x 50 μl) were made into the left ventricle. Animals were sacrificed 7 days following the procedure. Whole hearts were retrieved and assayed by spectroscopic absorption at 420nm to quantify the total amount of beta-galactosidase expressed. Absorption data are given below on the basis of both sample size (150 μl) and mg protein (determined using a standard protein assay). These data indicate that beta-galactosidase expression is higher for the injections containing beads.

	420nm absorption/150μl	β-gal (A420/mg protein)
Adenovirus	55.49 (51.74; 59.23)	4.0 (3.3; 4.6)
Adenovirus plus beads	93.03 (110.26; 75.79)	8.1 (9.0; 7.1)

[0065] Although various embodiments are specifically illustrated and described herein, it will be appreciated that modifications and variations of the present invention are covered by the above teachings and are within the purview of the appended claims without departing from the spirit and intended scope of the invention.